

ANNULUS FIBROSIS AUGMENTATION METHODS AND APPARATUS

REFERENCE TO RELATED APPLICATIONS

This application is a continuation-in-part of U.S. patent application Serial No. 10/120,763, filed April 11, 2002, which is a continuation-in-part of U.S. patent application Serial Nos.:

- 5 09/807,820, filed April 19, 2001, which is a 371 of PCT/US00/14708, filed May 30, 2000;
 09/638,241, filed August 14, 2000;
 09/454,908, filed December 3, 1999, now U.S. Patent No. 6,491,724;
 09/639,309, filed August 14, 2000, now U.S. Patent No. 6,419,702;
- 10 09/690,536, filed October 16, 2000, now U.S. Patent No. 6,371,990, which is a continuation-in-part of U.S. patent application Serial Nos. 09/638,726, filed August 14, 2000, now U.S. Patent No. 6,340,369; and 09/415,382, filed October 8, 1999, now U.S. Patent No. 6,419,704.

The entire content of each application and patent is incorporated herein by reference.

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FIELD OF THE INVENTION

This invention relates generally to human spinal surgery and, in particular, to methods and apparatus for augmenting the annulus fibrosis while controlling vertebral motion, thereby preventing additional annular tears and attendant discomfort.

BACKGROUND OF THE INVENTION

20 According to human anatomy, spinal function is dependent upon the intervertebral disc and the facet joints. In a sense, the annulus fibrosis, nucleus pulposus, and the facet joints form the legs of a three-legged stool.

To restore disc height resulting, for example, from degenerative disease, prosthetic discs are used to replace only the nucleus pulposus. Reference is made to my

U.S. Patent No. 6,419,704, which discusses spinal anatomy, spinal physiology, disc degeneration, surgical and non-surgical treatments of disc disease, and the advantages of prosthetic disc replacement.

The annulus is formed of 10 to 60 fibrous bands which serve to control vertebral motion. One half of the bands tighten to check motion when the vertebra above or below the disc are turned in either direction. Restoring disc height returns tension to the annular noted in the prosthetic disc patent application. In addition, restoring annular tension decreases annular protrusion into the spinal canal or neural foramen. Thus, decreasing annular protrusion may eliminate pressure on the spinal cord or nerve roots.

At times the rotational, translational, and axial compression forces exceed the strength of the annular fibers. The excessive forces tear the annular fibers. A single event can tear one band to all the bands. Subsequent tears can connect to previous tears of a few bands resulting in a hole through the entire annulus fibrosis. Holes through the entire annulus fibrosis can result in extrusion of the nucleus pulposus. Extrusion of the nucleus pulposus is referred to as a "herniated disc." Disc herniation can result in back pain, neck pain, arm pain, leg pain, nerve or spinal cord injury, or a combination of the above.

Since the annulus is innervated with pain fibers, acute annular tears without herniation of the nucleus can be painful. Unfortunately, the annular tears often do not heal completely. The chronic tears can result in neck pain, back pain, shoulder pain, buttock pain, or thigh pain. The chronic tears weaken the annulus fibrosis predisposing the disc to herniation or additional annular tears. My U.S. Patent No. 6,340,369, entitled "Treating Degenerative Disc Disease With Harvested Disc Cells and Analogies of the Extracellular Matrix," and U.S. Patent No. 6,419,704, entitled "Artificial Intervertebral Disc Replacement Method And Apparatus" describe methods and apparatus for occluding annular defects.

Prosthetic replacement of the nucleus pulposus alone risks future problems arising from annular tears. Patients may continue to complain of pain from the stresses placed onto the weakened annulus. Secondly, tears of the annulus could result in extrusion of

the prosthetic nucleus. In addition, remaining nucleus pulposus could herniate through annular tears.

Some prosthetic disc designs attempt to replace nucleus and annular functions. In general, these designs attach the prosthetic disc to the vertebrae. Many of the techniques 5 in this area attach the prosthetic disc to the end plates of the vertebrae with screws, spikes, flanges, or porous surfaces for bone ingrowth. My U.S. Patent Nos. 6,245,107 and 6,419,704 describe methods and devices to assist the annulus in retaining remaining nucleus pulposus and a prosthetic nucleus. The entire contents of these applications are incorporated herein by reference.

10 The need remains, however, for a more extensive annulus augmentation technique. Failure at the disc vertebra interface could result in loosening of the prosthesis, however, and patients with loose prosthetic discs would likely require revision surgery.

SUMMARY OF THE INVENTION

15 The invention reconstructs the annulus fibrosis using methods and devices similar to those used in reconstruction of the ACL of the knee. Tendon (allograft or autograft) or tendon connected to bones (allograft or autograft) is grafted across the disc space and into the vertebrae. The grafts can be held in position with interference screws. The screws could be resorbable. The reconstructed annulus would a) help to control the movement 20 between the vertebrae, for example, rotation, translocation, and bending; and b) help prevent the extrusion of devices or material from the disc space.

A shape-changing material, clamp or cable tie may also be used to increase the height of an intradiscal device according to the invention. Additional fixation features may be added around a hoop or band to enhance surface area or prevent "pull-out."

25 BRIEF DESCRIPTION OF THE DRAWINGS

FIGURE 1 is a sagittal cross-section of the spine and the novel tendon graft;
FIGURE 2 is a lateral view of the spine and cross-coupled tendon grafts;

- FIGURE 3 is a lateral view of the a tendon graft;
- FIGURE 4 is a lateral view of a bone-tendon-bone graft;
- FIGURE 5 is a lateral view of a bone-tendon graft;
- FIGURE 6 is a lateral view of a bone-annulus-bone graft where the bone is from
5 the vertebral body;
- FIGURE 7 is a view of the posterior aspect of the spine with the novel tendon
graft;
- FIGURE 8A shows a lateral view of the way in which an allograft or autograft
tendon may be connected to bones across a disc space and into the vertebra;
- 10 FIGURE 8B shows an anterior view of the embodiment of Figure 8A;
- FIGURE 9A illustrates a tendon-bone composite according to the invention;
- FIGURE 9B illustrates an annulus-vertebrae composite;
- FIGURE 10 illustrates an alternative embodiment wherein a synthetic material
such as Gortex is used as opposed to tendon;
- 15 FIGURE 11A illustrates the way in which a hoop can be placed into a disc for
repair purposes;
- FIGURE 11B shows the hoop being inserted through the hole in the annulus;
- FIGURE 11C shows the hoop expanded within a disc space;
- FIGURE 12A illustrates a different embodiment wherein a bag containing nucleus
20 or synthetic materials such as hydrogel are inserted into a previously implanted hoop;
- FIGURE 12B is a drawing that shows a second step associated with the procedure
of Figure 12A;
- FIGURE 12C shows the way in which intradiscal materials are placed into a band
or hoop;
- 25 FIGURE 12D shows the way in which a hoop may change space to hold
intradiscal materials into position;
- FIGURE 12E is a drawing which shows the way in which a clamp or cable tie
may be used to increase the height of an intradiscal device;

FIGURE 12F shows how an intradiscal device is made taller through the tightening of a cable or clamp;

FIGURE 13A is a drawing which shows additional fixation features;

FIGURE 13B shows the fixation features of Figure 13A in a tightened position;

5 FIGURE 14 shows how a hoop or band could have ridges or grooves to prevent a suture from sliding;

FIGURE 15 illustrates an intradiscal device having openings on the top and/or bottom to insert a biocompatible material;

FIGURE 16A illustrates a wire frame without an outer shell;

10 FIGURE 16B is a side-view drawing of the device of Figure 16A; and

FIGURE 17 shows the use of a lever-like tool for center-filling purposes.

DETAILED DESCRIPTION OF THE INVENTION

This invention is broadly directed to reconstruction of the annulus fibrosis. Preferred embodiments use methods and devices similar to those used in reconstruction 15 of the ACL (anterior cruciate ligament) of the knee. Tendon (allograft or autograft) or tendon connected to bones (allograft or autograft) is grafted across the disc space and into the vertebrae. Alternatively, synthetic materials, such as Gortex, may be used for the reconstruction. The grafts can be held in position with interference screws that may be resorbable. Appropriate grafts may be obtained from cadaver's Achilles tendon, tensions 20 of the hamstring muscles, palmaris longus tendon, fascia, annulus fibrosis, patellar tendons, or other muscles, tendons, or ligaments of the body.

Figure 1 is a sagittal cross-section of the spine and a tendon graft 102 according to the invention. The tendon material is shown at 104 and the screws at 106, 108. Figure 2 is a lateral view of the spine and cross-coupled tendon grafts.

25 Figure 3 is a lateral view of a tendon graft. Figure 4 is a lateral view of a graft including bone 402, tendon 404, and bone 406. Figure 5 is a lateral view of a bone-tendon graft having a threaded portion 502. Figure 6 is a lateral view of a bone-annulus-bone graft where the bone portions 602, 604 are from the vertebral body. Figure 7 is a

view of the posterior aspect of the spine including a tendon graft according to the invention.

Figure 8A shows a lateral view of the spine showing the way in which an allograft or autograft tendon 802 may be connected to bones across a disc space 804 and into the 5 vertebra 806, 808. Procedurally, holes 810, 812 are formed in to the vertebral bodies, using drills, burrs or other conventional means, after which the tendon is inserted in either end and held in position with interference screws such as 820. Figure 8B shows an anterior view of the embodiment of Figure 8A.

Figure 9A illustrates a bone-tendon-bone (902-904-906) composite according to 10 the invention. Figure 9B illustrates a vertebrae-annulus-vertebrae (912-914-916) composite. Figure 10 illustrates an alternative embodiment wherein a synthetic material such as Gortex 1002 is used as opposed to tendon or annulus material.

Alternative embodiments of the invention use hoops or bands to fortify the annulus. Figure 11A illustrates the way in which a hoop 1102 can be placed into a disc 15 1104 through an annulus 1100 for repair purposes. Figure 11B shows the hoop being inserted through the hole in the annulus using an inserter tool 1110. Figure 11C shows the hoop expanded within the disc space. A shape-memory material may be useful for this purpose.

Figures 12A-12D illustrate a different embodiment, wherein a deformable 20 intradiscal component is made taller using a band of material that constricts due to a shape change. In Figure 12A, a hoop is inserted into the disc space. In Figure 12B, an intradiscal component, such as a bag containing nucleus or synthetic materials such as hydrogel is inserted into the previously implanted hoop. In Figure 12C, the hoop is slid over the bag, and in Figure 12D, the hoop changes shape to hold intradiscal materials into 25 position and/or increase the ratio of height to width of an intradiscal device.

Figure 12E is a drawing which shows the way in which a clamp or cable tie 1202 may be used to increase the height of an intradiscal device 1204. A radiator-like clamp or a cable tie could also be used to increase the height of the bag and make the filled bag

firmer. Figure 12F shows how an intradiscal device is made taller within a disc space 1210 through the tightening of a cable or clamp.

Additional fixation features such as sutures 1302 and buttons 1304 may be added around a hoop or band 1306, as shown in Figure 13A, to enhance surface area or prevent 5 “pull-out.” Figure 13B shows the fixation features of Figure 13A in a tightened position. Figure 14 shows how a hoop or band could have ridges or grooves 1402 to prevent a suture from sliding.

Figure 15 illustrates an intradiscal device 1500 having openings 1502, 1504 on the top and/or bottom (or a through-hole) to insert a biocompatible material 1510.

10 Figure 16A illustrates the use of a wire frame comprising an outer ring 1604 and an inner ring 1606 without an outer shell. Figure 16B is a side-view drawing of the device of Figure 16A. Vertical supports 1610 may be used between the rings. The wire frame is collapsible to insert the device through an annular window. The frame re-expands vertically and circumferentially once in the disc space. The front of the device 15 can be compressed to insert material after it is positioned in the disc space.

The vertical supports help to keep the bag expanded vertically, and the top and bottom contain an opening to insert material and to aid diffusion. The outer covering could be any biocompatible fabric or mesh. The inner frame would have spring-like properties but could also have other shape memory properties. Figure 17 shows how a 20 lever-like tool 1702 may be used to collapse the front 1704 of the device to fill the center, after which the device expands to trap the material.

I claim: